



Brain-Computer Interfaces for 1-D and 2-D Cursor Control: Designs using Volitional Control of the EEG Spectrum or Steady-State Evoked Potentials



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Context and Relevance to NASA Missions





Problem

- Increasing mental and physical demands in long-duration human exploration
- Adverse and restricted environments, risk of fatigue, exhaustion, overload

Goals

- New interfaces for mobile or restricted environments
- Augmented interaction in normal environments
- Increased bandwidth / multi-tasking
- Quickening the interface
- Enhanced situational awareness
- Increased mission safety and reliability by early detection of adverse states and adaptive automation

Context and Relevance to NASA Missions

Projects

- Voluntary control of EEG (mu-rhythm) for cursor control
- SSVEP-based BCI for handsfree control of displays (moving maps)
- Mental state estimation

Recent Advances

- Feature selection
- Classification algorithms
- On-line adaptation





Challenges

- Artifact removal
- Training methods
- Contactless sensors

Electroencephalography 101 Basis of EEG



Biophysical Basis of Voluntary EEG Control

(Desynchronization of µ-rhythm)



(Adapted from Beatty, 1995)

Target Practice



PLS-based EEG Processing

- We regard the power spectral density of single EEG epochs of C channels and F spectral lines as a vector \mathbf{x} (*M*), with $\mathbf{M} = \mathbf{C} \times \mathbf{F}$ dimensions.
- Each x_i (i = 1, 2, ..., n) is a row vector of a matrix of explanatory variables, X (n × M), with M variables and n observations.
- The n observations are the power spectral densities or PSDs of single EEG epochs from two classes, (e.g., experimental conditions, alert/fatigued, etc.).

PLS-based EEG Processing

- We regard the class membership of each EEG epoch as a matrix Y (n × 1) in which Class 1 is assigned the value 1 and Class 2 is assigned the value -1.
- PLS models the relationship between the explanatory variables and class membership by decomposing **X** and **Y** into the form

 $\mathbf{X} = \mathbf{T}\mathbf{P}^T + \mathbf{F}$ $\mathbf{Y} = \mathbf{U}\mathbf{Q}^T + \mathbf{G}$

- T and U are matrices of p extracted score vectors (components),
- **P** and **Q** are matrices of loadings
- **F** and the $(n \times M)$ matrix **G** are matrices of residuals.

PLS-based EEG Processing

- PLS maximizes the covariance between the components of the explanatory variables and class membership.
- We use the nonlinear iterative partial least squares algorithm (NIPALS), which finds weight vectors **w**, **c** such that $max_{|\mathbf{r}| = |\mathbf{s}| = 1}[cov(\mathbf{Xr}, \mathbf{Ys})]^2 = [cov(\mathbf{Xw}, \mathbf{Yc})]^2 = [cov(\mathbf{t}, \mathbf{u})]^2$
- cov(t, u) = t^Tu/n denotes the sample covariance between the score vectors t and u.
- Application of the weight vectors to normalized data produces component scores that serve as inputs to a classifier.
- We have tested both discretized linear regression (DLR) and support vector classifiers (SVC).

On-line PLS EEG Processor



Biophysical Basis of Steady-State VEP

Repetitive patterned visual stimulation produces a frequency-following (or doubling) response in primary visual cortex, which is easily recorded by occipital EEG electrodes.



Demo from David Heeger's lab at NYU http://www.cns.nyu.edu/~david/fmri-demos/V1MTmovie.mpg

SSVEP-based BCI



On-line PLS EEG Processor



Successful demonstrations of 1-D and 2-D control

- Voluntary control of EEG
- SSVEP based BCI
- On-line adaptive feature extraction/classification Future applications
- Telerobotics
- Virtual or restricted environments
- Restricted environments
- Disabled personnel